University of Wisconsin Madison





# CT Contrast Agents and Enhancement

**Principles** 

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#### CONFLICT OF INTEREST

No Conflict of interest to declare.

#### TEACHING POINTS

- 1. Learn about the major types of contrast agents used in CT: why they work and their clinical applications
- 2. Understand the route IV contrast agents take through the body: speed of travel, changes in enhancement, and commonly used imaging phases
- 3. Review the factors that influence CT contrast agent enhancement

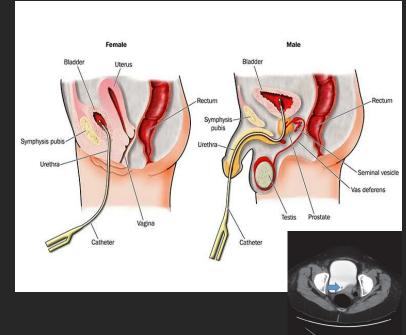
#### DIFFERENT TYPES OF CONTRAST AGENTS IN CT

CT contrast agents make soft tissue contrast in CT

**ORAL** 

CONTRAST

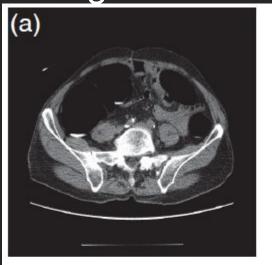


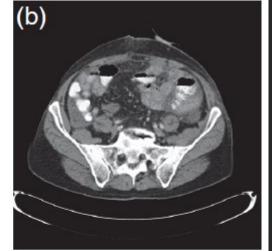


#### CT CONTRAST 101-NEGATIVE AGENTS

CO2 gas contrast agent

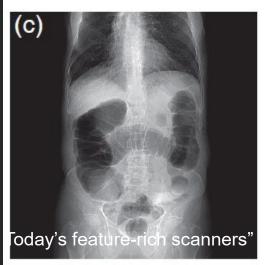
Same pt no CO2





Both scans have positive oral agent

Note: the localizers even show the CO2





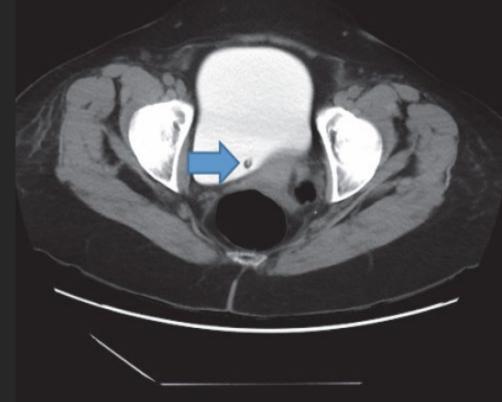
"The CT Handbook: Optimizing Protocols for Today's feature-rich scanners"

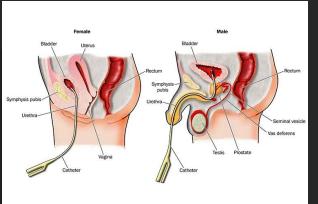
## CT CONTRAST 101-POSITIVE AGENTS

Positive agents are Iodinated contrast media (ICM)

Positive oral contrast introduced via Foley catheter

(arrow shows catheter, don't confuse this with an artifact)

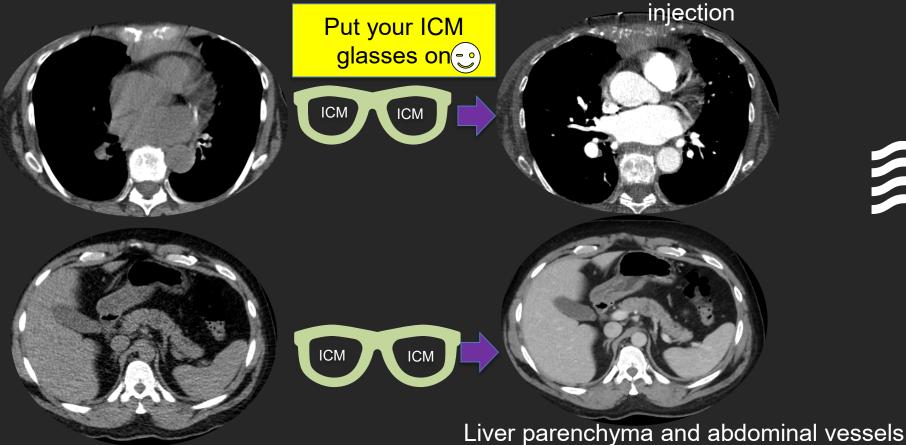




https://www.ausmed.com/cpd/articles/urinary-catheter

#### CT CONTRAST 101

Positive IV contrast (ICM) introduced through intravenous injection



Chambers and vessels of

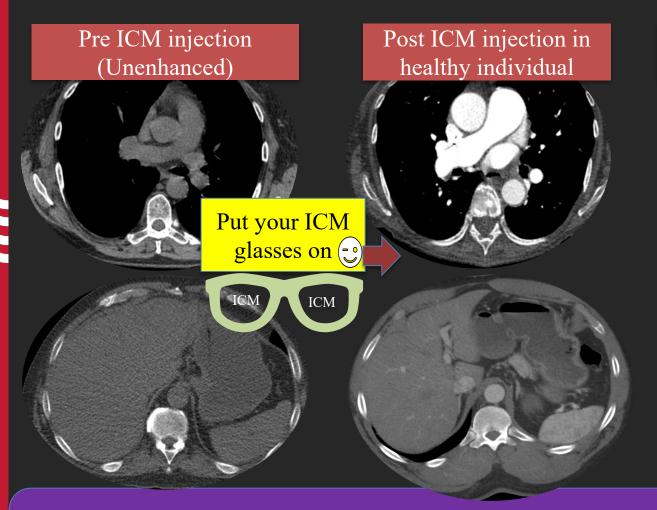
the heart and

mediastinum are better

visualized after ICM

are better visualized after ICM injection

# Most common application of ICM in CT is vascular (e.g. CT angiography) and visceral enhancement (e.g. parenchymal scan)



Post ICM injection in patient with pulmonary embolism

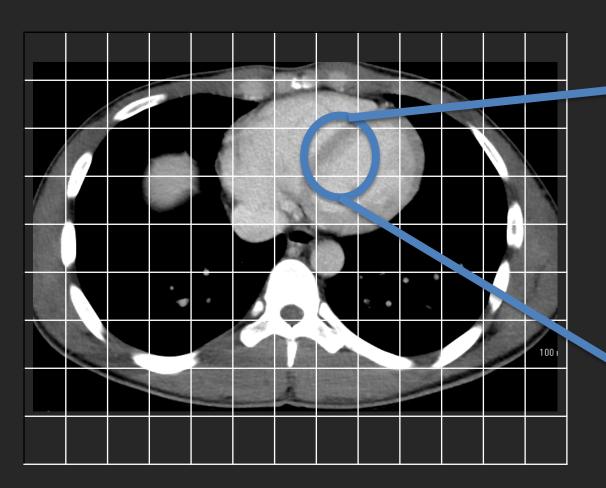
patient with HCC

A segment of the pulmonary artery remains unopacified due to pulmonary embolism, clearly visible following ICM injection.

Hepatocellular carcinoma is detectable only after ICM injection

Usually, it will always be diluted by blood (IVC administration) or water (oral) or urine (catheter injection)

#### WHY CONTRAST AGENTS WORK?



$$CT number = \frac{\mu - \mu_w}{\mu_w} \times 1000$$

linear attenuation coefficient of each voxel normalized by linear attenuation coefficient of water

<sup>1.</sup> Jiang, Hsieh. "Computed tomography: principles, design, artifacts, and recent advances." Bellingham, Washington USA (Published by SPIE and John Wiley & Sons, Inc.): SPIE 2009: 39-44.

Szczykutowicz T. The CT handbook: optimizing protocols for today's feature-rich scanners. Medical Physics Publishing, Madison WI. 2020: 282-289.

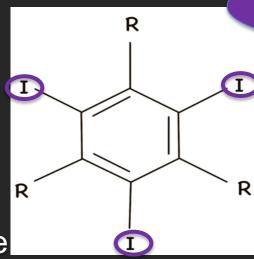
#### Positive ICM agent:

• 
$$\mu(\vec{X}, E) = \tau_{PE}(\vec{X}, E) + \sigma_{Compton}(\vec{X}, E)$$

$$= K\rho_e(\vec{X}) \frac{Z^3(\vec{X})}{E^3} + \rho_e(\vec{X}) f_{KN}(E)$$

$$Z_{l}=53$$
  
 $Z_{eff of water}=7.42$ 

Increased CT number when voxel contains iodine



3 lodine atoms per contrast molecule



#### Negative gas agent:

$$= K \rho_e(\vec{X}) \frac{Z^3(\vec{X})}{E^3} + \rho_e(\vec{X}) f_{KN}(E)$$

Decreased CT number when voxel contains CO2 due to low mass density and electron density

Iohexol is a common CT ICM and in different concentrations

Common concentrations of ICM used for diagnostic CT in the USA is 300-370 mgl/ml.

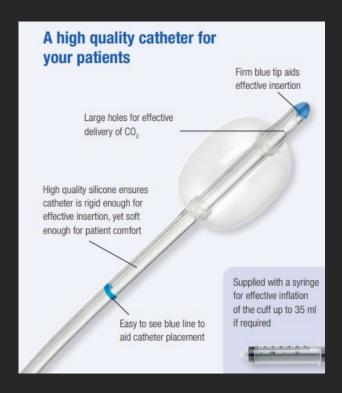
# Most common application of CO2 in CT is patients with allergy to ICM and poor renal function used in both arteriography and venography



Air/CO2

Generates CT number ~-1000, "usually doesn't get diluted"

Used for CTC



Images from "Automated Carbon Dioxide Insufflation System for Virtual Colonoscopy" by Bracco sales brochure

## IV INJECTION OF ICM



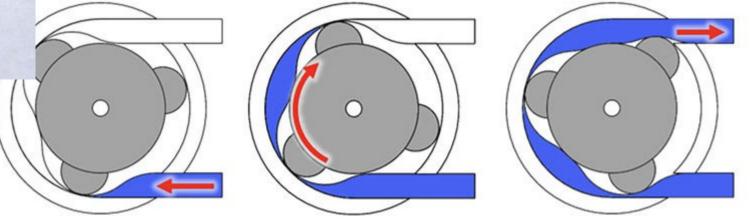


## CT CONTRAST 101



Piston based pump... simple, the plunger pushes the agent out

Peristaltic pump, the rotating action pushes agent along a flexible tube



https://dienerprecisionpumps.com/positive-displacement-pumps/

#### THE ROUTE OF IV CONTRAST AGENTS

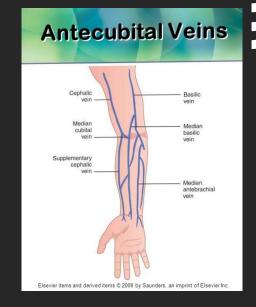
3. Blood goes to right ventricle and goes out pulmonary artery to lungs

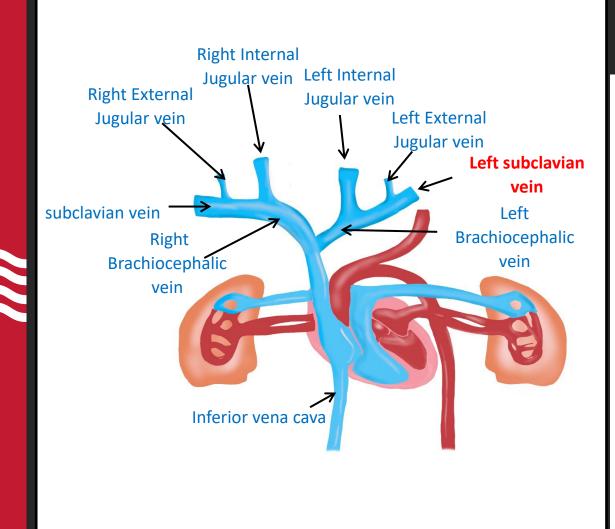
4. Returns via pulmonary vein and goes to left side of heart to be pushed out aorta via left ventricle.

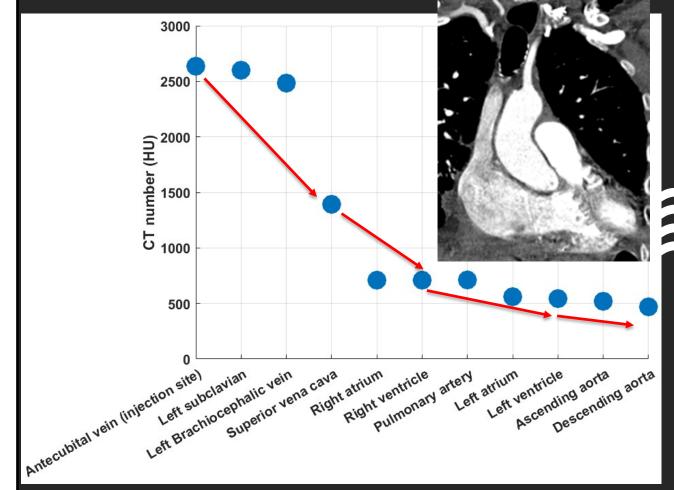
5. First stop is supplying heart via coronaries. Then head via carotid and vertebral vessels.

2. Blood goes into SVC and then into right atrium

1. Inject via antecubital vein







#### SPEED OF ICM TRAVEL

Contrast time of arrival will vary from person to person, but assuming an antecubital injection, values will generally be in the range of

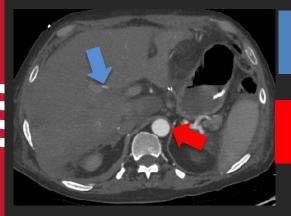
7 to 10 seconds for the pulmonary artery, 12 to 15 seconds for the ascending aorta, 15 to 18 seconds for the abdominal aorta, and 30 to 40 seconds for hepatic parenchyma.

Text copied from "The CT Handbook: Optimizing Protocols for Today's feature-rich scanners" By Tim Szczykutowicz. Medical Physics Publishing 2020

Another reference Bae, K. T., J. P. Heiken, and J. A. Brink. (1998). "Aortic and hepatic contrast medium enhancement at CT. part i. prediction with a computer model." *Radiology* 207(3):647–55.

#### COMMONLY USED IMAGING PHASES

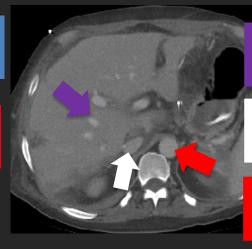
#### Arterial phase



Intrahepatic artery

Aorta

#### Venous phase

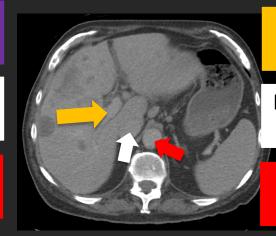


Hepatic vein

Inferior vena cava

Aorta

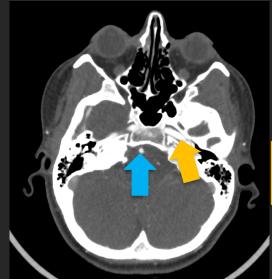
#### Delayed phase



Portal vein

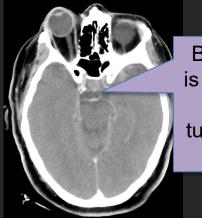
Inferior vena cava

Aorta



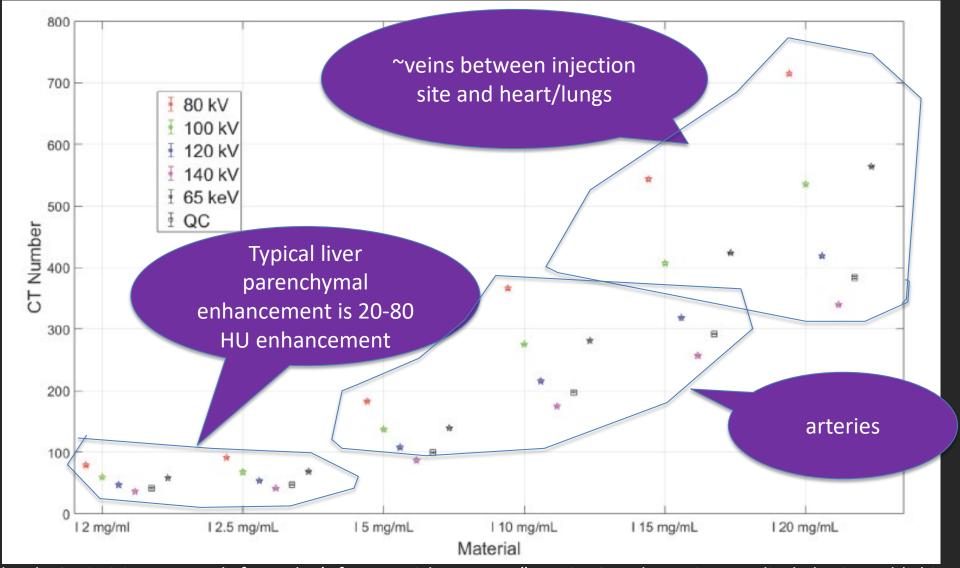
Basilar artery

Carotid artery



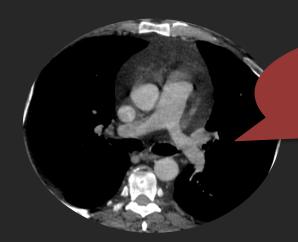
Brain parenchyma is homogenous with edge enhanced tumor (e.g. pituitary tumor)

#### CT CONTRAST 102





#### Examples of Good and Poor Contrast Enhancement



174 kg patient received 96 ml volume of ICM→ poor enhancement



Same patient repeated
with 159 ml volume of
ICM→ good
enhancement
More ICM→ more
enhancement

Larger volume of ICM results in higher contrast enhancement so why not give more ICM!?

**Acute adverse** 

allergic reactions

physiologic reactions

**Delayed effects** 

Mild

Moderate

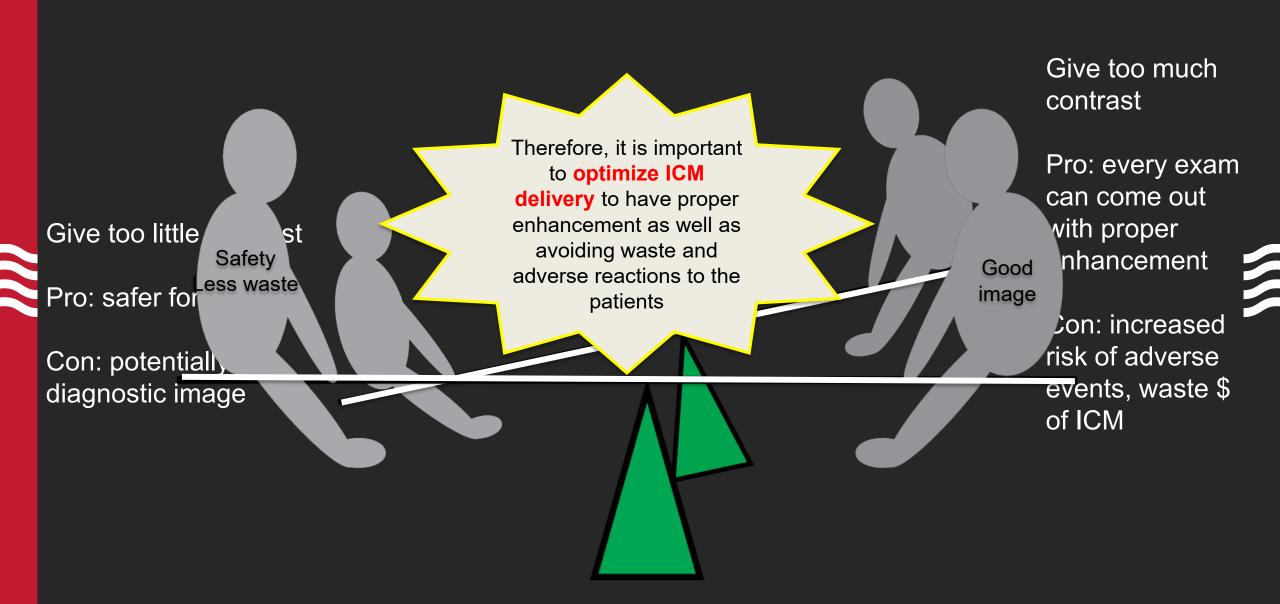
Severe

Contrast-induced acute kidney injury (CI-AKI)

- Clinical demand for ICMs will
- Environmental and Huk

Therefore, it is important to optimize ICM delivery to have proper enhancement as well as avoiding waste and adverse reactions to the patients

- 1. ACR manual on contrast media, 2024
- Preventing Future Global Shortages of Iodinated Contrast Media | GE HealthCare (United States) (https://www.gehealthcare.com/insights/article/preventing-future-global-shortages-of-iodinated-contrast media-requires-industry-action, Accessed 21st Jun 2024)
- 3. Cavallo JJ, Pahade JK. Practice management strategies for imaging facilities facing an acute iodinated contrast media shortage. American Journal of Roentgenology. 2022 Oct 13;219(4):666-70.
- 4. England A, Rawashdeh M, Moore N, Young R, Curran G, McEntee MF. More sustainable use of iodinated contrast media–Why?. Radiography. 2024 Jun 1;30:74-80.



#### Factors Affecting Iodine Contrast Enhancement

Following is a list of factors affecting iodine contrast enhancement in CT:

# Physics-based factors

- √ Tube potential
- √ Beam hardening
- √ Scan duration

## Patient-related factors

- √ Blood volume
- ✓ Cardiac output

#### Contrast Protocolbased factors

- ✓ Contrast volume
- ✓ Injection rate
- ✓ lodine concentration
- √Scan timing (scan delay)
- √ Saline flush

#### Tube Potential (kV)

ray spectrum

**Effective energy=** 

45 keV

Tube

potential= 80 kVp

80 100 120 140

Energy (kV)

lodine Water 80 kV acquisition X-10<sup>0</sup>

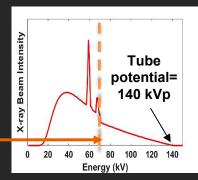
60 70 80

Photon Energy (KeV)

120

140 kV acquisition X-ray spectrum

**Effective energy=** 67 keV



 $\mu(\vec{X}, E) = \tau_{PE}(\vec{X}, E) + \sigma_{Compton}(\vec{X}, E)$ 

$$= K \rho_e(\vec{X}) \frac{Z^3(\vec{X})}{E^3} + \rho_e(\vec{X}) f_{KN}(E)$$

Larger difference between linear attenuation coefficient of lodine and water at 80 kV (lower energy)→ **Increased contrast** 

CT number (HU)

- Jiang, Hsieh. "Computed tomography: principles, design, artifacts, and recent advances." Bellingham, Washington USA (Published by SPIE and John Wiley & Sons, Inc.): SPIE 2009: 39-44.
- Szczykutowicz T. The CT handbook: optimizing protocols for today's feature-rich scanners. Medical Physics Publishing, Madison WI. 2020: 282-289.







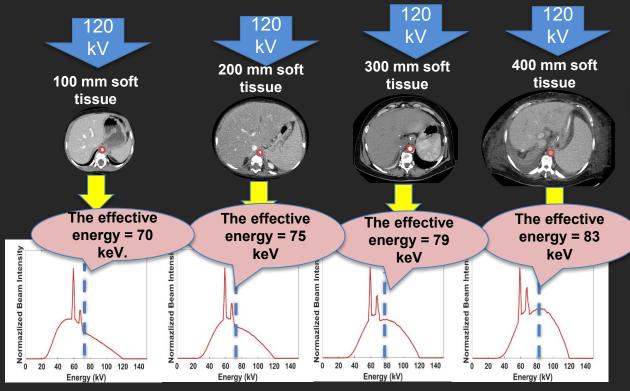


Beam energy (kV)

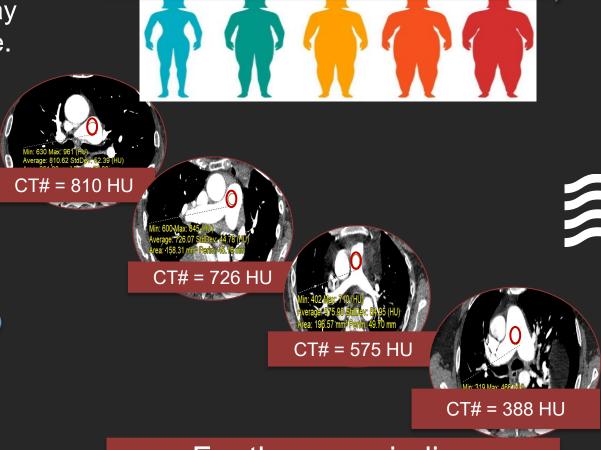
Material	80 kV	100 kV	120 kV	140 kV	N/A
Water	0	0	0	0	[-4 4]**
Air	-1,000	-1,000	-1,000	-1,000	[-1005 -995]**
Fat	-152*	-111*	-89*	-69*	[-100 -80]**
Brain	47*	43*	39*	37*	
Soft Tissue	62*	58*	54*	52*	
Solid Cortical Bone	3,760*	2,590*	1,940*	1,330*	[≈200 > 1000]**
Pure Calcium	9,570*	5,960*	3,950*	2,090*	
Pure Iodine	405,000*	267,000*	180,000*	93,200*	
Iodine Contrast	See footnote a	See footnote a	See footnote a	See footnote a	
Relative Iodine Enhancement <sup>b</sup>	1.68	1.27	1	0.826	
Relative Iodine Enhancement⁰	1.70	1.28	1	0.81	
Kidney					[20 40]**
Pancreas					[30 50]**
Blood					[50 60]**
Liver					[50 70]**
PMP					-200***
Low-Density Polyethylene					-100***
Polystyrene					-35***
Acrylic					120***
Delrin®					340***
Teflon®					990***

### Beam Hardening (BH) Related to Patient Size

Beam hardening: the gradual increase of average x-ray beam energy as it passes through more patient tissue.



- lodine concentrations in the ROIs (central circles) are identical
- Low energy X-rays are more attenuated by a larger patient

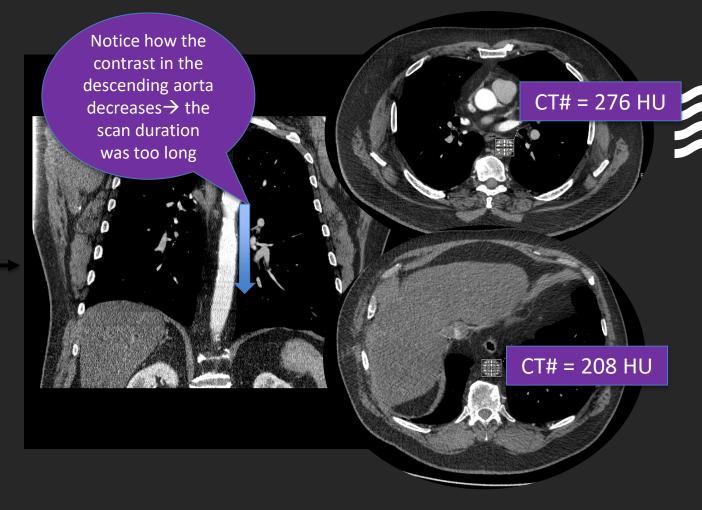


For the same iodine concentration, CT number drops with patient size.

### SCAN DURATION

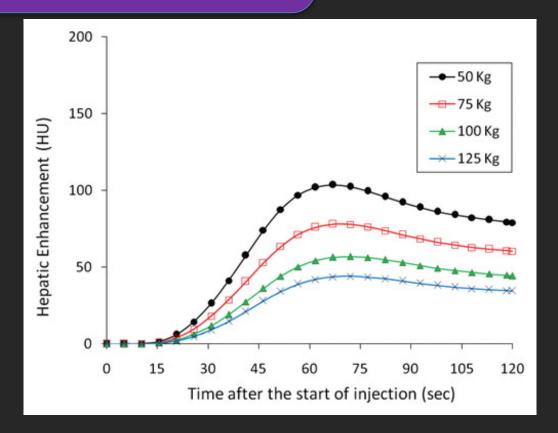
**Short scan duration** CT# (HU) Long scan duration Time (s)

Shorter scan duration should have slightly longer scan delays, so to coincide with maximum contrast enhancement



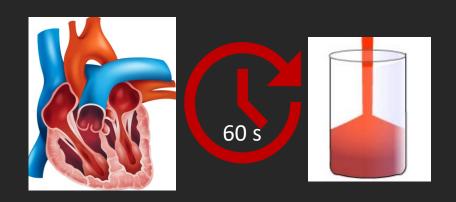
### **BLOOD VOLUME**

Blood volume effect: Bigger people have more blood... which dilutes contrast agent



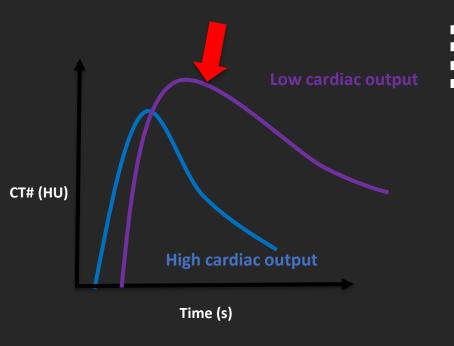
#### CARDIAC OUTPUT

Cardiac output: the volume of blood pumped by the heart in a 60 s interval.



Low cardiac output → circulation of ICM slows, ICM arrives and clears slowly → delayed time to peak enhancement

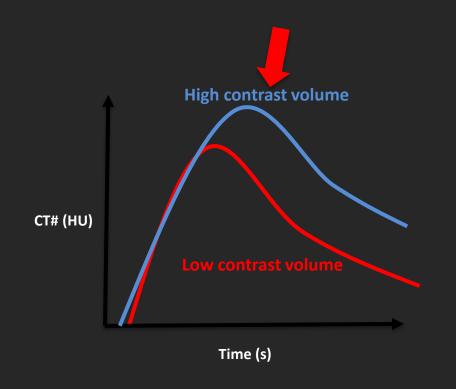
Low cardiac output  $\rightarrow$  Contrast enhancement increases because less un-opacified blood mixes with ICM when the cardiac output is low



### CONTRAST VOLUME

High contrast volume → high peak arterial enhancement

High contrast volume with fixed injection rate → increased time to peak enhancement



<sup>1.</sup> Holmquist F, Hansson K, Pasquariello F, Björk J, Nyman U. Minimizing contrast medium doses to diagnose pulmonary embolism with 80-kVp multidetector computed tomography in azotemic patients. Acta radiologica. 2009 Jan 1;50(2):181-93

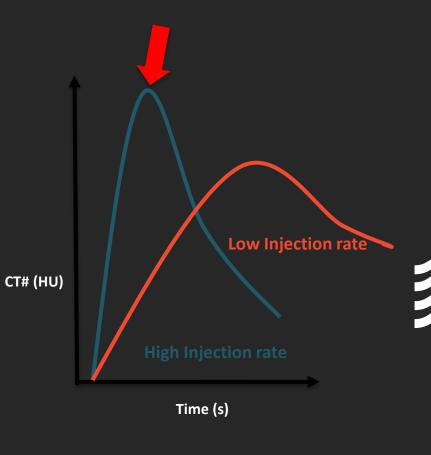
#### INJECTION RATE

High injection rate  $\rightarrow$  Increased peak arterial enhancement

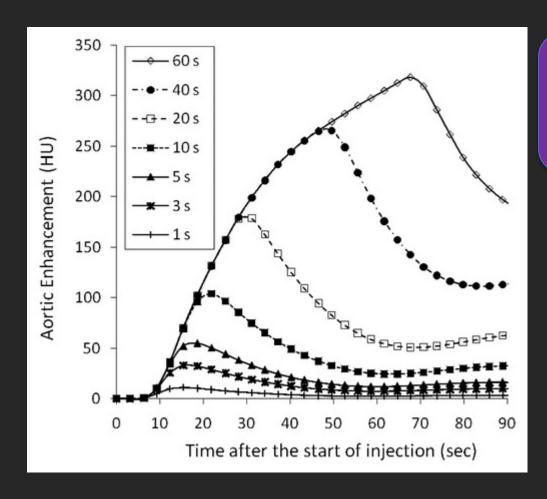
High injection rate  $\rightarrow$  Decreased time to peak arterial enhancement.

Higher injection rate  $\rightarrow$  Reduces potential temporal window for CT scanning (i.e., peak of contrast plateau is shorter)

For delayed phases, injection rate has little to no effect on enhancement



#### INJECTION DURATION



Injection duration effect: Longer and longer injections push CT enhancement up and delay peak enhancement

Arterial enhancement is "in and out" faster relative to parenchymal

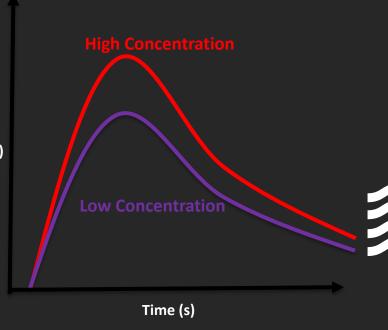
#### IODINE CONCENTRATION

We usually use higher concentration ICM for arterial studies.

Change in enhancement is equal to the ratio of the change in contrast agent concentration if everything else is held fixed.

CT# (HU)

If we change ICM concentration and keep the volume fixed, the total iodine mass to the patient changes proportional to the change in ICM concentration.



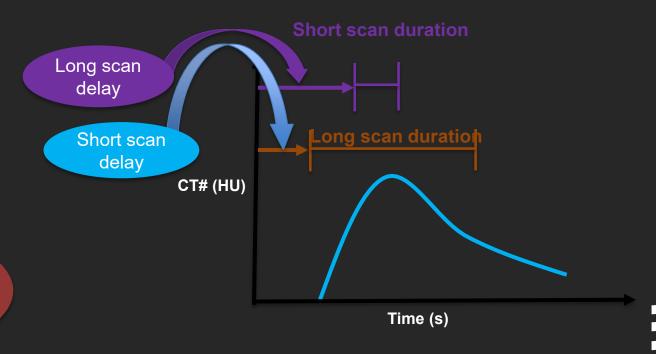
#### Scan Delay

Optimal Scan Delay = 
$$T_{Peak} - \frac{1}{2}T_{scan duration}$$

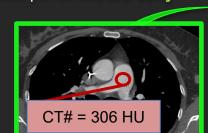
Anatomy and indication specific (i.e., for abdominal CTA this may be from an ROI in the aorta, for parenchymal liver it would be an ROI in liver)

Peak enhancement need to be optimized based on optimal enhancement time and scan duration

If scan delay is not set properly, peak enhancement can be missed.

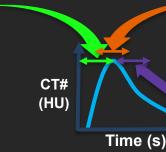


Well-timed CT pulmonary angiography



CT pulmonary angiography

was performed too early





CT pulmonary angiography was performed too late

- Bae KT. Intravenous contrast medium administration and scan timing at CT: considerations and approaches. Radiology. 2010 Jul;256(1):32-61
- 2. Szczykutowicz T. The CT handbook: optimizing protocols for today's feature-rich scanners,



#### SALINE FLUSH

Saline flush is a saline injection immediately following a contrast injection.

We can think of the flush as "saline pushing the contrast" as opposed to using "contrast to push the contrast" from injector to the heart.

Usually used on CTA exams to make sure iodine is not wasted and left in veinous system.

This is why we see a benefit for CTA exams and little benefit for parenchymal phase exams.

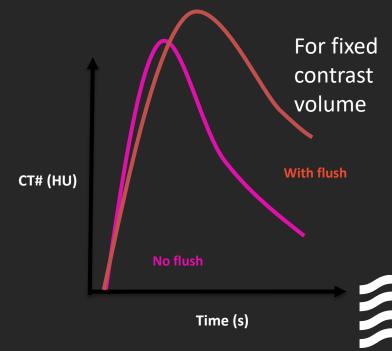
Use of 20-30 ml of saline flush leads to a 5-10% increase in peak arterial enhancement.

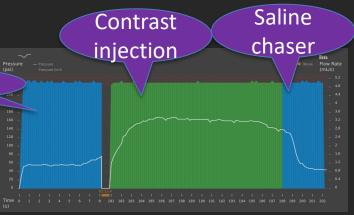
Contrast can be reduced with use of a flush.

When we use a flush, we see a prolonged time to peak arterial HU compared to non-flush.

test injection

It can reduce ICM streak artifact issues when ICM is left in high concentrations in SVC or other vessels in a patient's arm or upper thorax.





- 1. Bae KT. Intravenous contrast medium administration and scan timing at CT: considerations and approaches. Radiology. 2010 Jul;256(1):32-61.
- 2. Lee CH, Goo JM, Bae KT, Lee HJ, Kim KG, Chun EJ, Park CM, Im JG. CTA contrast enhancement of the aorta and pulmonary artery: the effect of saline chase injected at two different rates in a canine experimental model.

  Investigative radiology. 2007 Jul 1;42(7):486-90
- 3. Behrendt FF, Bruners P, Keil S, Plumhans C, Mahnken AH, Das M, Ackermann D, Günther RW, Mühlenbruch G. Effect of different saline chaser volumes and flow rates on intravascular contrast enhancement in CT using a circulation phantom. European journal of radiology. 2010 Mar 1:73(3):688-93

#### Equations Governing the Major Facets of Contrast Delivery

$$Volume_{arbitrary strength}(ml) = \frac{Strength_{reference}(mg I / ml)}{Strength_{arbitrary}(mg I / ml)} Volume_{reference strength(ml)} [See Table 8.2]$$

$$Volume(ml) = Duration(s) \times Injection flow rate(ml / s) [See Table 8.3]$$

 $Total\ iodine\ load\ (mg\ I) = Contrast\ concentration\ (mg\ I\ per\ ml) \times Contrast\ volume\ (ml)$ 

Scan delay = Time to optimal enhancement  $-\frac{1}{2}$  Scan duration

$$Scan speed (mm/s) = \frac{Collimation (mm) \times Pitch}{Rotation time (s)}$$

$$Scan duration(s) = \frac{Scan range(mm)}{Scan speed(mm / s)}$$

$$= \frac{Scan range(mm) \times Rotation time(s)}{Collimation(mm) \times Pitch}$$

Contrast volume as a function of patient weight and contrast strength is shown in Table 8.3 for routine abdominal parenchymal enhancement.

#### **Equations Governing the Major Facets of Contrast Delivery**

$$Volume_{arbitrary strength}(ml) = \frac{Strength_{reference}(mg I / ml)}{Strength_{arbitrary}(mg I / ml)} Volume_{reference strength(ml)} [See Table 8.2]$$

$$Volume(ml) = Duration(s) \times Injection flow rate(ml / s)$$
 [See Table 8.3]

 $Total\ iodine\ load\ (mg\ I) = Contrast\ concentration\ (mg\ I\ per\ ml) \times Contrast\ volume\ (ml)$ 

Iodine load versus contrast volume

All volumes are not created equal... a lower volume of high concentration agent can deliver the same total lodine as a larger volume of less concentrated agent

Want more enhancement?
Increasing volume can give more
enhancement, but change contrast timing

Increasing concentration will increase enhancement and usually wont change timing

#### Scan delay = Time to optimal enhancement $-\frac{1}{2}$ Scan duration

$$Scan speed (mm/s) = \frac{Collimation(mm) \times Pitch}{Rotation time(s)}$$

$$Scan duration(s) = \frac{Scan range(mm)}{Scan speed(mm / s)}$$

$$= \frac{Scan range(mm) \times Rotation time(s)}{Collimation(mm) \times Pitch}$$





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